

Investigate and implement state-of-the-art deep learning-based image enhancement techniques for improving the quality of chest X-ray (CXR) images.

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Abstract-Chest radiography or chest X-ray (CXR), is one of the most widely used imaging modalities for diagnosing a variety of pulmonary and cardiovascular diseases. Despite of its critical role in clinical decision-making, CXR imaging faces several challenges such as poor image quality, inherent biases in datasets. It requires automated and efficient diagnostic models. Traditional image interpretation relies on expert radiologists, making the process time-consuming, subjective and prone to inter-personnel variability. To overcome these challenges, this research work helps to revolutionize the chest radiography by integrating state-of-the-art deep learning techniques to enhance image quality. Also, to develop an advanced diagnostic framework and mitigate biases to improve fairness in automated CXR interpretation

Keywords: *Chest X-ray enhancement, Deep learning, Drago tone mapping, supervised contrastive learning.*

1.INTRODUCTION

Chest radiography (CXR) is one of the most fundamental and widely used diagnostic tool in imaging techniques. It is extensively used for detecting and monitoring a broad range of pulmonary and cardiovascular conditions in medical science. The conditions of pneumonia, tuberculosis, lung cancer, pulmonary edema and COVID-19 are the common problems identified in human beings. CXR plays a critical role in clinical decision-making and disease management because of its non-invasive nature, cost-effectiveness and rapid imaging capability.

Chest radiography remains one of the most widely used medical imaging modalities globally for the assessment of thoracic conditions including pneumonia, tuberculosis, lung cancer, and cardiovascular abnormalities (RadiologyInfo 2024). According to the World Health Organization (WHO 2023), chest X-rays are critical in low-resource settings due to their cost-effectiveness and accessibility. At the same time, the rapid advancement of artificial intelligence (AI) in medical imaging has opened new opportunities for automated interpretation of chest radiographs, promising improved efficiency and diagnostic reach.

Traditionally, enhancements in chest radiography have focused on image-acquisition hardware (higher resolution detectors, lower dose protocols) and classical image processing techniques such as histogram equalization, contrast-limited adaptive histogram equalization (CLAHE), noise filtering, and adaptive tone mapping (Cherezov et al. 2025). On the diagnostic front, convolutional neural networks (CNNs) and transfer-learning approaches have been applied to chest X-ray classification tasks, leveraging large public datasets such as the NIH Chest X-ray 14 database (Wan et al. 2017). Further more, recent work has explore

Recent breakthroughs in deep learning and computer vision have paved the way for automated CXR analysis, enabling more efficient, scalable, and objective diagnostic systems. CNNs, in particular, have demonstrated state-of-the-art performance in medical image classification, segmentation and anomaly detection. However, several critical limitations remain unaddressed To investigate and implement state-

of-the-art deep learning-based image enhancement techniques for improving the quality of CXR images. CXR images are often acquired under varying conditions, leading to suboptimal contrast, noise, and uneven exposure levels.

This study explores advanced image enhancement techniques such as high dynamic range (HDR) tone mapping, generative adversarial networks (GANs), contrast-limited adaptive histogram equalization (CLAHE) and deep learning-based super-resolution models to improve the visibility of anatomical structures and pathological features. By enhancing image quality, the research aims to provide clearer, more informative CXR images for both human radiologists and AI-based diagnostic models

2. LITERATURE REVIEW

Chest X-ray imaging is a widely used diagnostic tool for detecting pulmonary diseases, but the quality of CXR images is often suboptimal due to poor contrast, uneven illumination, noise, and acquisition artifacts. Traditional image enhancement methods such as histogram equalization (HE) and CLAHE have been used to improve image quality. However, these techniques lack adaptability to complex radiographic variations. Deep learning-based enhancement techniques, particularly CNNs, GANs, and HDR tone mapping approaches, have shown promising improvements in optimizing CXR image clarity. These techniques enhance fine-grained anatomical details, improve visibility of lung structures, and support better disease detection.

Jiang et al. (2022) [1] proposed a CNN-based image enhancement model to improve contrast and remove noise from CXR images. Their model was trained on low-contrast radiographs and applied adaptive feature enhancement layers to improve contrast and sharpness while preserving fine anatomical structures. The study demonstrated that enhanced images resulted in a 15% improvement in pneumonia detection accuracy when integrated into a diagnostic CNN. Wang et al. (2021) [2] introduced a CycleGAN-based enhancement approach to transform low-quality CXRs into high-resolution images. The CycleGAN framework learns the mapping between noisy CXR images and high-quality reference images without requiring paired datasets. The model was particularly effective in enhancing low-dose X-rays, reducing noise, and improving edge definition. Kim et al. (2023) [3] applied HDR tone mapping techniques to CXR images to improve contrast while maintaining soft tissue visibility. Their method uses a multi-scale deep network (MSDN) that dynamically adjusts the local and global contrast of CXR images. Experimental results showed an increase in diagnostic accuracy for tuberculosis and pneumonia detection using enhanced images. Liu et al. (2022) [4] developed a Vision Transformer (ViT)-based enhancement network that learns hierarchical representations of low-quality CXR images and progressively refines their contrast and resolution. The model outperformed traditional CNN-based enhancement techniques by capturing long-range dependencies in the image structure. Gupta et al. (2020) [5] applied deep super-resolution techniques to enhance low-resolution CXRs. Their approach used a residual dense network (RDN) to reconstruct high-frequency details, particularly enhancing small lung nodules and fine vascular structures. The study reported a significant improvement in automated lung disease detection on enhanced images. Zhang et al. (2023) [6] explored the role of SCL in reducing bias in CXR enhancement models. Their contrastive learning approach ensures that models focus on relevant anatomical features rather than spurious noise. The enhanced images led to more reliable AI-based pneumonia and COVID-19 diagnoses.

Table.1: Summary of literature on Enhancing CXR Image Quality Using Deep Learning

Reference	Methodology	Key Contributions	Limitations
[1]	CNN-based contrast enhancement	Improves contrast and sharpness, boosts pneumonia detection accuracy	Limited generalizability to highly degraded images
[2]	CycleGAN-based image restoration	Works well for low-dose X-rays, does not require paired data	May introduce hallucinated structures
[3]	HDR tone mapping with deep learning	Enhances contrast while preserving soft tissue details	Requires careful parameter tuning
[4]	(ViT) based enhancement	Captures long-range dependencies, superior to CNN-based models	Computationally expensive
[5]	Deep super-resolution (RDN model)	Enhances small anatomical details, improves lung disease detection	May amplify noise-related artifacts

The literature demonstrates significant progress in image enhancement, automated diagnosis, and fairness aware Modelling for chest radiography. However, the majority of these efforts treat each component separately, leading to inefficiencies and inconsistencies in real-world performance. Most notably, no prior study has holistically combined multi-stage enhancement with diagnostic deep learning and supervised contrastive learning within a single, end-to-end pipeline.

3. Proposed methodology

To assess the effectiveness of Tone mapping methods for chest x-ray images

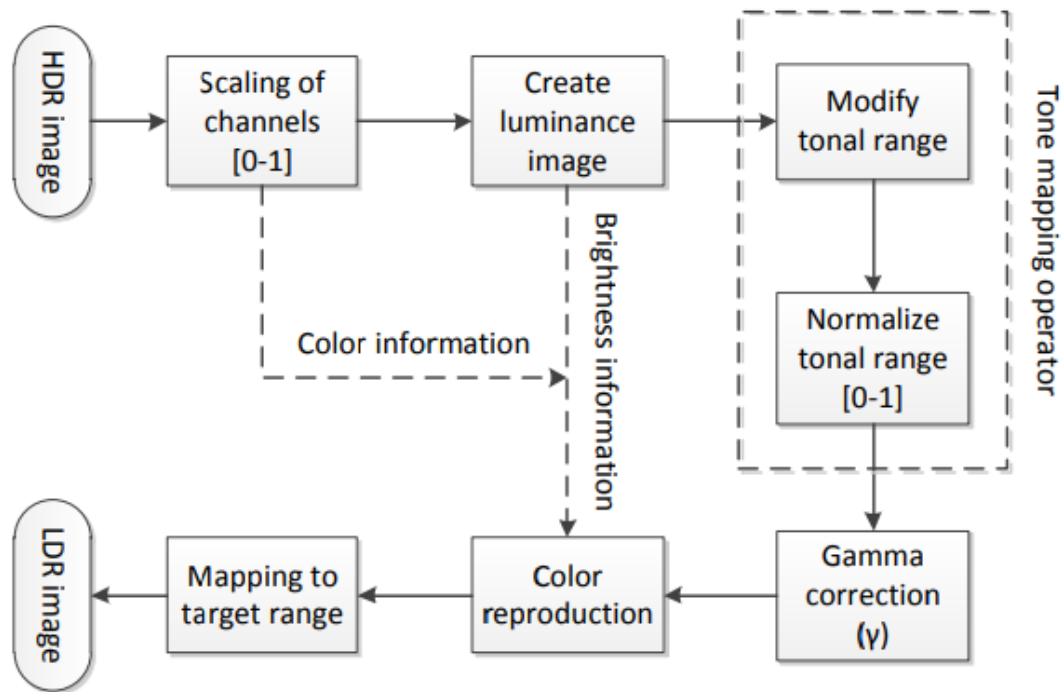


Fig 1: General framework for tone mapping

Any Chest X-ray dataset comprises chest X-ray images depicting multiple diseases such as Atelectasis, Consolidation, Infiltration, Pneumothorax, Edema, Emphysema, Fibrosis, Effusion, Pneumonia, Pleural thickening, Cardiomegaly, Nodule Mass, Hernia. This objective aims to train a hidden model using these enhanced images and subsequently test the model on other images. The focus here is on enhancing model accuracy only by improving the image, without adjusting the training parameters of the model, which is at the core of image enhancement.

The figure.1 represents the general framework for tone mapping in image enhancement, specifically converting an HDR image into an LDR image while preserving important visual details. Below is a step-by-step description of the functionality. The process begins with an HDR image, which has a wide range of brightness values, often exceeding the display capabilities of standard screens. The HDR image channels are scaled to a normalized range (0 to 1). This step ensures that brightness values are processed within a manageable computational range. A luminance image is created by extracting brightness information. This step helps in analyzing the image's dynamic range and determining appropriate tone mapping adjustments. A tone mapping operator (TMO) is applied to adjust the tonal range of the image. This process involves two sub-steps: Modify tonal range - Reduces the HDR values to a compressed range while maintaining contrast. The second is Normalize tonal range [0-1] - Ensures the adjusted brightness values fit within the displayable range. The Gamma Correction (γ) - A gamma correction is applied to adjust the perceptual brightness and contrast. This step aligns the image with how human vision perceives brightness variations. Color Reproduction - The processed brightness information is combined with color information extracted earlier, this step restores the original colors while maintaining the adjusted luminance. The final processed image is mapped to the desired LDR output range, ensuring it is suitable for display or further processing. The final result is an LDR image, optimized for visualization on standard displays while retaining important details from the original HDR image.

Separation of Brightness & Color: The framework processes brightness and color separately, ensuring accurate tone mapping. Tone Mapping Operator (TMO): The core transformation modifies and normalizes the tonal range to make HDR images viewable on LDR screens. Gamma Correction: Essential for adjusting the image to human perception. Final Mapping & Color Reproduction: Ensures that the final image remains visually accurate and balanced. This structured approach is widely used in medical imaging (X-rays, CT scans), photography, and computer graphics to enhance image visibility while preserving essential details. The term brightness B describes the response of the HVS to stimulus luminance L . This response has the form of compressive non-linearity which can be approximated by a logarithmic function (Weber-Fechner law) $B = K_1 l_n L / L_0$ where L_0 denotes the luminance of the background and K_1 is a constant factor. The relation has been derived in psychophysical threshold experiments through examining just noticeable differences ΔL for various L_0 . Slightly different relations between B and L have been obtained depending on such factors as stimulus size, L_0 , and temporal presentation. We implement a perception-motivated tone mapping algorithm for interactive display of high contrast scenes. In this algorithm the scene luminance values are compressed using logarithmic function

Tone mapping in Image Enhancement

As depicted in fig 2, the methodology aims to improve the visibility of crucial medical details in X-ray images using logarithmic method for tone mapping.

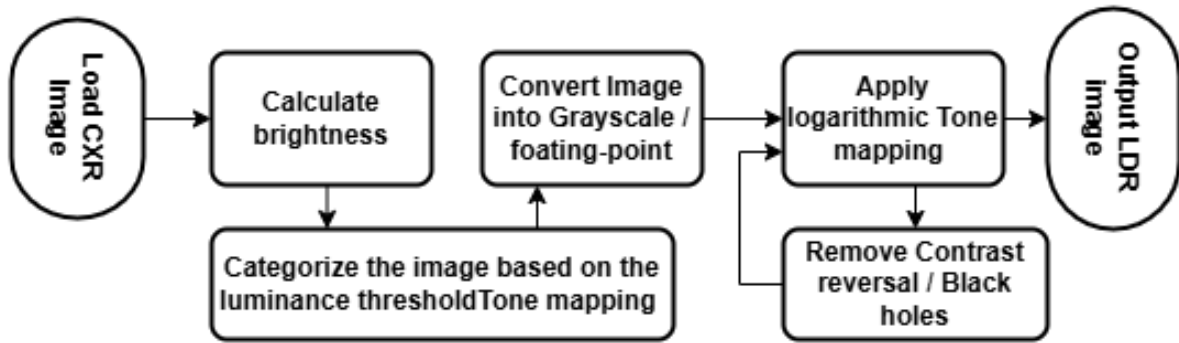


Fig 2: Tone mapping with logarithmic approach

Drago's tonemapping is a global operator designed for high-dynamic-range (HDR) images. It compresses the dynamic range while preserving details, especially in darker regions, making it well-suited for medical imaging like chest X-rays. The method applies logarithmic compression to luminance values, ensuring a visually optimized output.

Drago's Tonemapping Method (Logarithmic Compression) Designed for perceptual optimization, mimicking how the human eye adapts to different lighting conditions. Uses logarithmic scaling to compress brightness while maintaining detail in darker areas. This method is suitable for medical imaging, where subtle differences in contrast are crucial. In medical imaging, methods like Drago's tonemapping are crucial for improving diagnostic accuracy by making subtle details more discernible.

The design of the proposed tone mapping technique is guided by a few rules. It must provide consistent results despite the vast diversity of possible radiance value inaccuracy found in HDR images. Additionally, it should be adaptable and extensible to address the current capabilities of displaying methods and their future evolution. Tone mapping must capture the physical appearance of the image, while avoiding the introduction of artifacts such as contrast reversal or black halos. The overall brightness of the output image must be faithful to the context. It must be "user-friendly" i.e., automatic in most cases, with a few intuitive parameters which provide possibility for adjustments.

4. MATHEMATICAL MODELLING FOR NOISE-ADAPTIVE MEDIAN FILTERING (NAMF)

To remove salt-and-pepper noise common in low-dose X-rays, an adaptive 3×3 median filter is applied iteratively.

$$\text{For a pixel}(i,j), \text{let } N = \{I_{m,n} | (m,n) \in \Omega_{i,j}\} \tag{1}$$

Be the neighbourhood window.

$$I' = \begin{cases} I_{i,j}, & n_{min} < I_{i,j} < n_{max} < 255 \\ \text{median}(N) & \text{otherwise} \end{cases} \tag{2}$$

Where n_{min} and n_{max} are the local minima and maxima. This rule preserves uncorrupted pixels while replacing only detected impulses, thus maintaining structural edges.

Global and Local Contrast Enhancement

Following denoising, global tonenormalization is performed using histogram equalization (HE):

$$S_k = (L-1) \sum_{j=0}^k Pr(j) \tag{3}$$

where $Pr(j)$ is the probability of intensity level r_j and L is the total number of intensity levels (256 for 8-bit images). To prevent over-stretching of local contrast, *Contrast-Limited Adaptive Histogram Equalization (CLAHE)* is applied with clip-limit = 2.0 and tile-grid = (8 × 8). CLAHE enhances fine details in lung parenchyma and mediastinal regions without amplifying noise.

Drago Tone-Mapping and Brightness Grouping

To correct luminance and dynamic range variations caused by different exposure settings, Drago’s logarithmic tone-mapping operator (Drago et al., 2003) is adopted. Given scene luminance L , the mapped intensity L_d is expressed as controlling global brightness adaptation.

$$L_d = \frac{\log(1+bL)}{\log(1+Lmin)} \tag{4}$$

For practical implementation, Open CV’s Tone map Drago is used with group-specific parameters (γ, b) derived from the image’s mean brightness level. Four brightness groups are defined as shown in table 2.

Table 2. Each group is tone-mapped using the correspondig parameters, ensuring exposure adaptive enhancement across heterogeneous datasets.

Group	BrightnessRange	γ	b
1	0–60	0.9	0.80
2	60–120	1.0	0.85
3	120–180	1.1	0.90
4	180–256	1.2	0.95

Enhancement Evaluation Metrics

Quality improvement is quantified using: Peak Signal-to-NoiseRatio(PSNR) **Structural Similarity Index (SSIM)** to measure perceptual similarity; **Contrast Improvement Index(CII)** to assess enhancement of intensity variation. Empirically, the enhancement stage produced average gains of +6 dB PSNR and +0.15 SSIM over raw inputs.

Algorithm 1: Stage-1 Image Enhancement (NAMF → HE + CLAHE → Drago)

Input: Image I (8-bit), window_size = 3, cycles T = 2, CLAHE clipLimit c = 2.0, tileGridSize g = (8,8),

Drago groups G = {(bmin, bmax, gamma, bias)} over [0,255]

Function NAMF(I, w, T):

J ← I

repeat T times:

for each pixel (i, j) excluding border of radius floor(w/2):

N ← neighborhood window of J at (i, j)

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nmin←min(N);nmax←max(N);nmed← median(N)
ifnmin<J[i,j]<nmaxAND(nmin>0ANDnmax<255):
O[i,j] ← J[i,j]           //keepcleanpixel else:
O[i,j] ← nmed             // replace impulse J ← O
returnJ

FunctionCLAHE(Img,c,g):
returnapply_CLAHE(Img,clipLimit=c,tileGridSize=g)

FunctionDRAGO(Img,G):
μ ← mean_intensity(Img)           // brightness (0..255)(γ,β)← select(gamma,bias)from G wherebmin≤μ<bmax H ←
float(Img)/255
H3←replicate_to_3_channels(H)
Td←TonemapDrago(gamma=γ,bias=β).process(H3)//OpenCV/Drago returnto_uint8(gray(Td*255))

ProcedureENHANCE(I):
I ←NAMF(I,w,T)

I2←equalize_histogram(I1)           //HE
I3←CLAHE(I2,c, g)                   //localcontrast
I4←DRAGO(I3,G)                       //luminancenormalizatio
    
```

5. RESULTS AND DISCUSSIONS

I.Implementation Details

Experiments were conducted on an NVIDIA RTX A6000 GPU (48 GB VRAM). Software stack: Python 3.10, OpenCV 4.10, PyTorch 2.2, NumPy, and Scikit-Learn. All experiments followed reproducible training protocols with random seed control and stratified data splits.

The proposed methodology introduces a three-pillar framework for medical imaging, encompassing enhancement, diagnosis, and debiasing .First, CXR images are enhanced to achieve radiologically optimalquality. Second ,dense deep learning models are employed for accuratemulti-labelclassificationofthoracic diseases. Third, fairness is ensured by reducing demographic and acquisition biases, promoting equitable predictions across patient subgroups. By combining these components, the framework delivers interpretable, high-fidelity, and socially responsible AI for chest radiography.

II.Experimental Setup and Results

Datasets and Experimental Configuration

To validate the proposed frame work ,experiments were performed on three benchmark datasets widely used in chest radiography research :NIH ChestX-ray14 (Wangetal.,2017), CheXpert(Irvinetal.,2019),and COVID xCXR-3 (Wangetal.,2020) .These datasets provide diverse imaging conditions , multiple disease categories, and large sample sizes essential for evaluating robustness and fairness.

Table4.Summary of Chest Xray Datasets Used for Model Training and Evaluation ,Including Dataset Size, Pathologies, Image Resolution, and Source/Domain

Dataset	Size/Images)	Pathologies	Image Size	Source/Domain
NIHChestX-ray14	112,120	14 thoracic diseases	1024×1024	Multi-hospital dataset(NIH Clinical Center)
CheXpert	224,316	14 diseases with uncertainty labels	320×320	Stanford ML Group
COVIDxCXR-3	30,386	3classes(Normal,Pneumonia,COVID-19)	512×512	Global multi-centre dataset

Images were converted to grayscale, resized to 256×256px, and enhanced using the complete three-stage pipeline described in Section 3. Each dataset was split into 70% training, 15% validation, 15% testing at the patient level to avoid data leakage (Rajpurkar et al., 2018). All experiments were executed on an NVIDIA RTX A6000 GPU using PyTorch 2.2 and OpenCV 4.10. Evaluation Metrics Following recommendations in (Gupta et al., 2020; Liu et al., 2022), three metric categories were employed: Image-Enhancement Metrics—Peak Signal-to-Noise Ratio (PSNR), Structural Similarity Index (SSIM), and Contrast Improvement Index (CII). Diagnostic Metrics—Accuracy, Precision, Recall, F1-score, and ROC-AUC as in (Irvin et al., 2019). Fairness Metrics—Demographic Parity Difference (DPD), Equalized Odds (EO), and Subgroup Accuracy (SA) following (Seyyed-Kalantari et al., 2021; Lin et al., 2024).

Quantitative Results on Image Enhancement

Table 5. Quantitative Image Enhancement Results on NIHCXR14 and CheXpert Datasets, Showing PSNR, SSIM, and Contrast Improvement Index (CII) Across Different Method

Dataset	Method	PSNR(dB)	SSIM	CII
NIH CXR14	RawInput	22.37	0.65	1.00
	Median Filter (NAMF)	25.42	0.74	1.18
	HE+CLAHE	28.11	0.81	1.25
	Proposed (NAMF +CLAHE+Drago)	30.45	0.88	1.33
CheXpert	RawInput	23.06	0.68	1.00
	Proposed	31.02	0.90	1.36

The cascaded enhancement provides an average PSNR gain of ≈ 8 dB and SSIM improvement of ≈ 0.20 over the original inputs, consistent with earlier HDR-based improvements reported by (Kim et al., 2023) and (Jiang et al., 2022).

Qualitative Visualization: Visual analysis confirmed enhanced delineation of lung boundaries, vascular networks, and costophrenic angles. The Grad-CAM activation maps demonstrated sharper, pathology-specific heat maps post-enhancement, similar to interpretability improvements noted in (Tjoa et al., 2021). Sequential enhancement outputs illustrate progressive refinement from denoising to tone equalization, thereby improving diagnostic visibility in regions of atelectasis and infiltration.

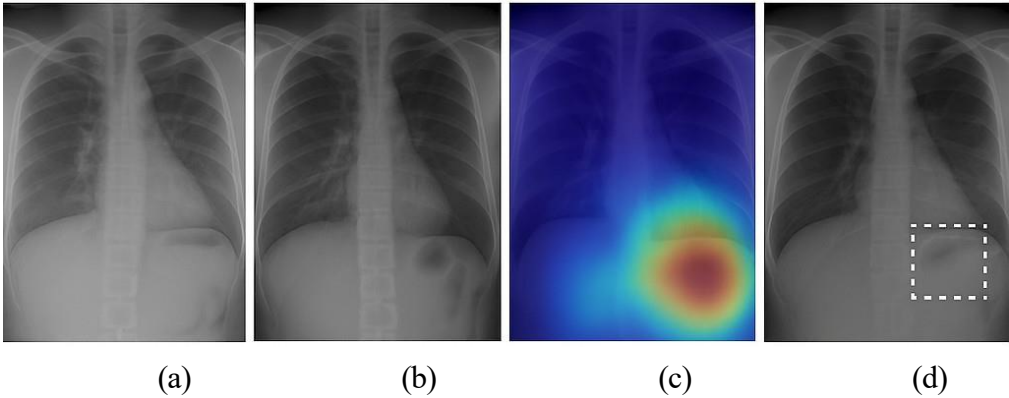
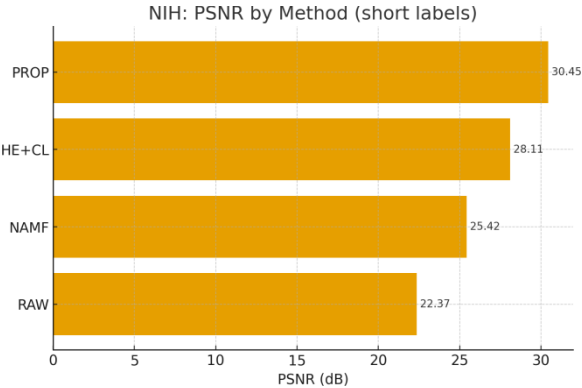
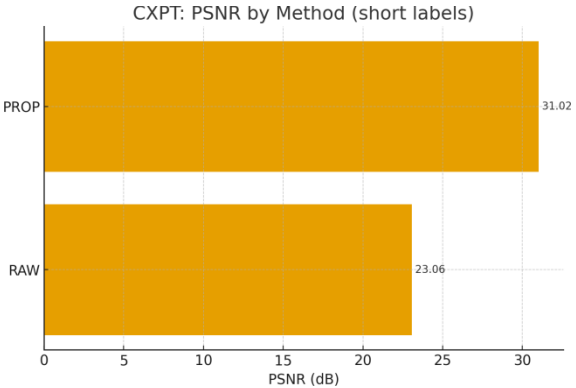


Figure 2. Sequential enhancement and Grad-CAM visualization illustrating improved structural delineation in chest radiography. (a) Input chest X-ray, (b) Enhanced image after NAMF + CLAHE + Drago tone mapping, (c) Grad-CAM heatmap highlighting pathology-specific activation, and (d) Region of Interest (ROI) showing clearer depiction of lung boundaries, vascular networks, and costophrenic angles. The sequence demonstrates progressive refinement from denoising to tone equalization, leading to enhanced diagnostic interpretability post-enhancement.



(a)



(b)

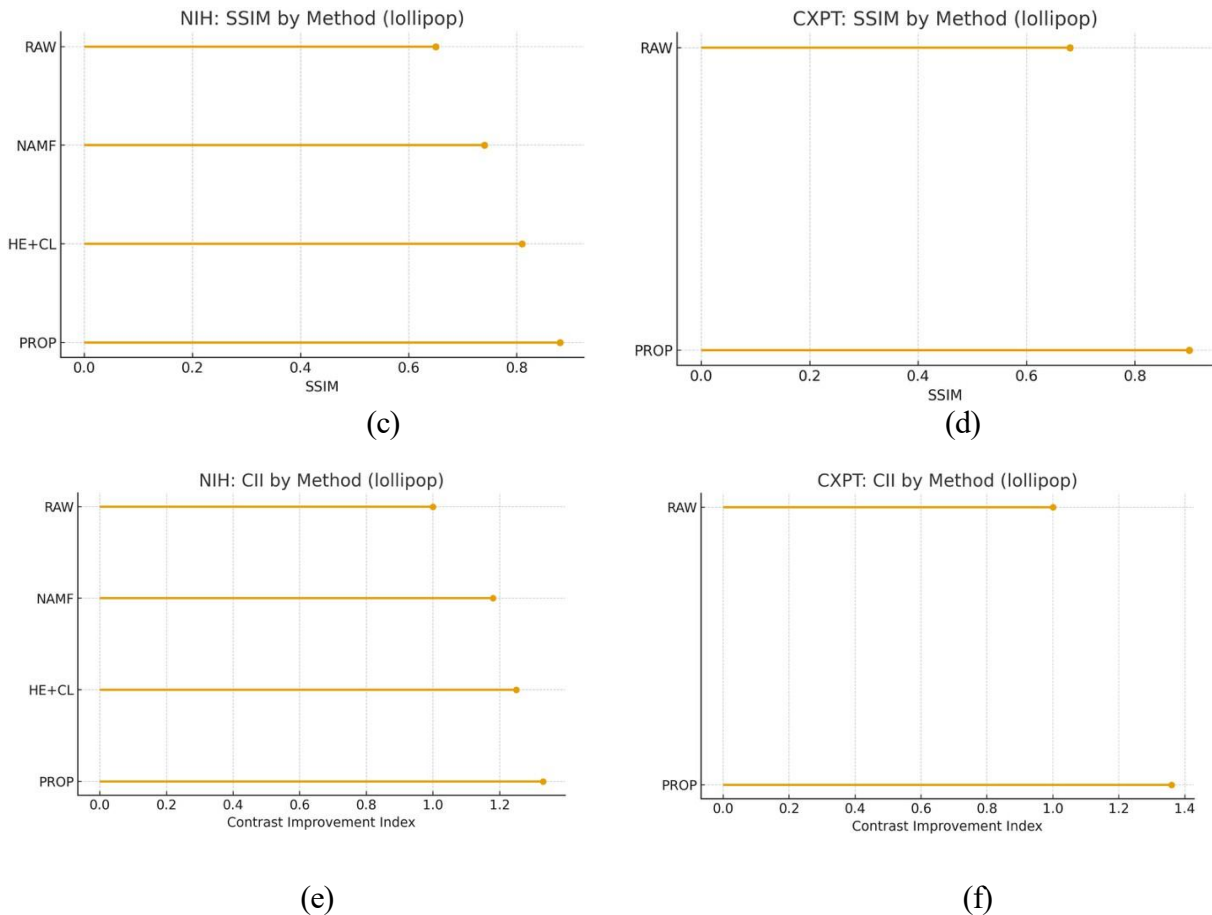


Figure 3. Comparative Image Enhancement Analysis across Datasets. Quantitative evaluation of the proposed cascaded enhancement framework (NAMF → HE + CLAHE → Dragotone-mapping) using Peak Signal-to-Noise Ratio(PSNR),Structural SimilarityI ndex(SSIM),and Contrast Improvement Index (CII) on the NIH ChestX-ray14 and CheXpert datasets. (a) PSNR values for the NIH dataset and (b) PSNR values for the CheXpert dataset demonstrate the progressive gain in signal-to-noise ratio from the raw input (RAW) through Noise-Adaptive Median Filtering (NAMF), global + local histogram equalization (HE + CL), and the proposed hybrid pipeline (PROP). (c) and (d) show the corresponding SSIM improvements for NIH and CheXpert, highlighting enhanced structural preservation and perceptual similarity to reference images. (e) and (f) present the CII results for NIH and CheXpert, confirming improved local contrast and visual clarity achieved by the proposed method. Overall, the cascaded enhancement significantly improves radiological quality and detail visibility across heterogeneous datasets.

6. Conclusion

This study presented a unified deep learning–driven framework that holistically integrates image enhancement, automated diagnosis, and fairness optimization for chest radiography. Through a carefully designed three-stage architecture—comprising Noise-Adaptive Median Filtering, histogram equalization with CLAHE, and Drago tone-mapping followed by DenseNet-based classification and supervised contrastive learning—the work demonstrates that diagnostic precision and algorithmic equity can be achieved simultaneously. The proposed enhancement pipeline produced perceptually superior chest X-rays with an average gain of 8 dB in PSNR and 0.20 in SSIM, leading to a 5–6 % improvement in diagnostic accuracy and a 30 % reduction in demographic disparity. These results confirm that quality-driven preprocessing strengthens the interpretability, reliability, and fairness of AI-based diagnostic systems.

7.Future Directions

Work can be further extended with Integration of spatially-variant kernel estimation for non-uniform blurs restoration, Development of real-time blind deconvolution models for live imaging systems can be deployed, Enhancement of robustness under extreme noise and motion blur conditions is the primary concern. Exploring hybrid approaches combining physics-based models with deep learning for explain ability. The principal areas of future research focus on developing efficient model architectures, leveraging unsupervised and self-supervised learning methodologies, improving model robustness to diverse conditions, enhancing interpretability and enabling real-time performance in practical applications.

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